Synthesis of Pore-Size-Tunable Mesoporous Silica Nanoparticles by Simultaneous Sol-Gel and Radical Polymerization to Enhance Silibinin Dissolution

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What's Known

• Silibinin, a major phytochemical of milk thistle seeds indicated in chronic liver disease and cirrhosis, exhibits low solubility and, consequently, low oral bioavailability.

• Mesoporous silica nanoparticles (MSNs) are intended for drug delivery due to their small pore size (2–50 nm), high specific surface area, excellent biodegradability, and biocompatibility.

What's New

• Synthesis of MSNs with tunable sizes and pore diameters was attained by simultaneous sol-gel reaction and free-radical polymerization.

• High capacity loading of silibinin in MSNs enhanced its dissolution and the preservation of its antioxidant activity in acidic gastric juice.

Abstract

Background: Silibinin (SBN), a major active constituent of milk thistle seeds, exhibits numerous pharmacological activities. However, its oral bioavailability is low due to poor water solubility. This study aimed to develop a new synthetic approach for tuning the pore characteristics of mesoporous silica nanoparticles (MSNs) intended for the oral delivery of SBN. In addition, the effects of the pore diameter of MSNs on the loading capacity and the release profile of SBN were investigated.

Methods: The present study was performed at Shiraz University of Medical Sciences, Shiraz, Iran, in 2019. This synthesis method shares the features of the simultaneous free-radical polymerization of methyl methacrylate and the sol-gel reaction of the silica precursor at the n-heptane/water interface. SBN was loaded onto MSNs, the *in vitro* release was determined, and the radical scavenging activities were compared between various pH values using the analysis of variance.

Results: According to the Brunauer–Emmett–Teller protocol, the pore sizes were well-tuned in the range of 2 to 7 nm with a large specific surface area ($600-1200 \text{ m}^2/\text{g}$). Dynamic light scattering results showed that different volume ratios of n-heptane/water resulted in different sizes, ranging from 25 to 100 nm. Interestingly, high SBN loading (13% w/w) and the sustained release of the total drug over 12 hours were achieved in the phosphate buffer (pH=6.8). Moreover, the antioxidant activity of SBN was well preserved in acidic gastric pH.

Conclusion: Well-tuned pores of MSNs provided a proper substrate, and thus, enhanced SBN loading and oral dissolution and preserved its antioxidant activity. Nevertheless, further *in vitro* and *in vivo* investigations are needed.

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Keywords • Nanoparticles • Silicon dioxide • Polymerization • Silybin • Antioxidants

Introduction

Among the compounds developed in the pharmaceutical industry, about 40% show low solubility or are completely insoluble. To improve the solubility and dissolution profile of such active agents, formulation scientists need to overcome several obstacles in different phases of formulation development.¹

Over the past decades, a plethora of different organic and inorganic nanoparticles were developed for drug delivery applications.² These materials have a great scope in the field of medicine, since they can show better pharmacokinetic and pharmacodynamic profiles. Nowadays, drug delivery based on inorganic nanomaterials such as gold nanoparticles, iron oxide nanoparticles, guantum dots, and mesoporous silica nanoparticles (MSNs) is the focal point of great scrutiny.³⁻⁵ Since the discovery of M41S in the early 1990s, MSNs with pore sizes ranging from 2 to 50 nm have attracted much attention, due to their unique properties such as high surface areas and pore volumes, uniform and tunable pore sizes, excellent biodegradability and biocompatibility, and easily modifiable surface properties.⁶ Moreover, great progress has been made in the multi-functionalization design and structure control of MSNs for their potential applications such as catalysis, adsorption, separation, sensing, and drug delivery.^{7,8} In recent years, MSNs have served as an emerging drug delivery system for various therapeutic agents.9 Silica is classified as "Generally Recognized as Safe" (GRAS), by the United States Food and Drug Administration (FDA), and is widely used in cosmetic, food, and pharmaceutical industries as rheology modifiers, suspending agents, and glidants. In addition, clinical trials are still performed with targeted silica nanoparticles for an image-guided operative sentinel lymph node mapping. In contrast to solid silica nanoparticles, a mesoporous structure allows a high drugloading capacity and a time-dependent drug release.^{3, 4} Internal silica nanochannels with large pore volumes can provide a high surface area for drug adsorption and loading, while silanolenriched external surfaces are easily-modified and enable sustained, controlled, targeted, and stimuli-responsive drug delivery to improve therapeutic drug efficacy.10 Shen and colleagues reported that the tunable pore size of MSNs could effectively control the loading and release kinetics of ibuprofen as a poorly water-soluble drug.11

MSN synthesis follows a self-assembly mechanism, whereby the physical, chemical, and structural properties of the nanoparticle are controlled by reactant ratios and experimental conditions. Recent innovations in the synthesis of MSNs with controlled particle size, morphology, and porosity, along with their chemical stability, have made silica an attractive biomaterial for drug delivery.^{3, 12, 13} Most often in the synthesis of MSNs, surfactants such as cationic cetyltrimethylammonium bromide

(CTAB) are employed owing to their strong association with silica precursors, which results in MSNs with small pore sizes (about 3 nm). On the other hand, many new applications of MSNs require uniform and large pore sizes in the range of 4 to 8 nm.³

Silibinin (SBN) is one of the structural isomers of the flavonoid silymarin, which is extracted from the milk thistle.14 Over the past two decades, SBN has received much attention due to its anticancer and chemopreventive actions, as well as its cholesterollowering, cardioprotective, and neuroprotective applications. SBN is a diastereoisomeric mixture of two flavonolignans, namely SBN A and SBN B, at a ratio of approximately 1:1.15 In contrast to the broad therapeutic actions of SBN, its bioavailability is limited due to low aqueous solubility, low permeability across intestinal epithelial cells, extensive phase II hepatic metabolism, and rapid excretion in the bile and urine.¹⁶ Moreover, the poor oral bioavailability of SBN is attributed to its degradation in the gastric fluid, which leads to more than a 20% degradation rate over 2 hours.17

The low solubility and possible inactivation of SBN in the gastrointestinal tract can impede the oral bioavailability of SBN, requiring drug incorporation into an efficient delivery system. Therefore, various approaches have been proposed, including drug encapsulation into liposomes, polymeric micelles, nanoparticles, prodrugs, and microspheres.¹⁶ It is assumed that MSNs with uniform and large pore sizes can provide a new platform for delivering poorly water-soluble phytochemicals such as SBN. For example, Cao and colleagues formulated a poorly water-soluble SBN based on polymeric porous silica nanoparticles,¹⁸ and Ahmadi Nasab and others prepared MSNs for the delivery of curcumin (a poorly water-soluble phytochemical).¹⁹ In light of the aforementioned research, we sought to develop well-tuned MSNs for SBN loading in high capacity with an enhanced drug dissolution rate. Unlike the conventional sol-gel method, the present MSN synthesis involves a combination of the hydrolytic condensation of tetraethyl orthosilicate (TEOS) to form silica and the simultaneous free-radical polymerization of methyl methacrylate (MMA) in a system of n-heptane/water dispersion. To optimize the delivery system, we studied the effects of the MSN pore size on the loading capacity and release profile of SBN. We also examined the impact of MSN encapsulation on preserving the antioxidant activity of SBN via the 2, 2-diphenyl-1-picrylhydrazyl (DPPH) radical scavenging assay.

Materials and Methods

The present study was performed at Shiraz University of Medical Sciences, Shiraz, Iran, in 2019. All the applied protocols were approved by the Research Ethics Committee of Shiraz University of Medical Sciences (Code: IRSUMS. REC.1397.1129).

Materials

TEOS (≥99%) (Merck, Germany), CTAB (Dae-Jung, South Korea), MMA, L-lysine (97%), 4,4'-Azobis (4-cyanovaleric acid) (ACVA), SBN (Sigma-Aldrich, U.S.A.), and n-heptane (Caledon, Canada) were used in the current investigation. Deionized water was produced using the MilliQ3 Integral 3 Water Purification System (Millipore, U.S.A.). All the chemicals were used as received.

Synthesis of Mesoporous Silica Nanoparticles

The synthesis method shares the features of the simultaneous free-radical polymerization of methacrylate ester and the sol-gel reaction of the silica precursor at the n-heptane/water interface (figure 1A). The process uses a basic amino acid as the catalyst, n-heptane as the organic phase component, ACVA as the initiator, and CTAB as the cationic surfactant. Briefly, 300 mg of CTAB was dissolved in 96 mL of deionized water. The mixture was purged with nitrogen gas for 45 minutes, at 70 °C. After a clear solution was obtained, different amounts of n-heptane (6 and 45 mL) were added to the solution. After 15 minutes, respective amounts of 0.5 and 20 mg/mL of MMA, 66 mg of L-lysine, 3000 mg of TEOS, and 0.81 mg/mL of ACVA were added to the reaction mixture, while it was stirred at 750 rpm (table 1). After four hours, the resulting



Figure 1: Schematic synthesis route is presented for the preparation of hybrid nanoparticles, composed of mesoporous silica and poly MMA. (A) FE-SEM micrographs correspond to the H1M1 (B) and H2M2 (C) preparations. MMA: Methyl methacrylate; FE-SEM: Field emission scanning electron microscopy; H1M1: A formulation prepared with 6 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 20 mg/mL of MMA

Table 1: Different MSN formulations, as well as Brunauer–Emmett–Teller and Dynamic light scattering results									
Sample	Reagent Variation	Mean Particle Size (nm)	Pore Size (nm)	Surface Area (m ² g ⁻¹)	Pore Volume (cm³ g⁻¹)	Silibinin Loading Capacity (%)			
H0M0 (Control)	Without adding n-heptane and MMA	106.0	2.40	1193.00	1.44	0.99			
H1M1	6 mL of n-heptane and 0.5 mg/mL of MMA	44.6	5.60	747.56	0.96	9.6			
H2M2	45 mL of n-heptane and 20 mg/mL of MMA	25.9	7.10	606.68	1.10	13.0			

MSN: Mesoporous silica nanoparticles; BET: Brunauer-Emmett-Teller; DLS: Dynamic light scattering; MMA: Methyl methacrylate; H0M0: A formulation prepared without adding n-heptane and MMA; H1M1: A formulation prepared with 6 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 20 mg/mL of MMA

product showed homogeneous milky colloidal dispersion. It was then cooled down to room temperature and decanted. The organic template and surfactant were removed by heating the raw products in an oven (500 °C) for five hours. The final product was kept in a desiccator until use. MSN products were characterized using field emission scanning electron microscopy (FE-SEM), the Brunauer-Emmett-Teller (BET) protocol, X-ray diffraction (XRD), and dynamic light scattering (DLS).

Characterization of Mesoporous Silica Nanoparticles

Field Emission Scanning Electron Microscopy The morphology and particle size of the gold-coated samples were characterized using FE-SEM (TESCAN, U.S.A.) operated at 15 kV.

Nitrogen Adsorption

The pore characteristics of the samples were studied by determining nitrogen adsorption isotherms using a surface area and pore size analyzer (Micrometrics, U.S.A.) at -196 °C through the BET protocol. Before the commencement of the experiment, the powder samples (≤200 mg) were transferred to a bulb and evacuated to a pressure of 10⁻⁴ Pa at 50 °C for 24 hours. The specific surface area was estimated from the nitrogen adsorption data over a relative pressure (P/P_0) , ranging from 0.0 to 1.0. Pore size distributions and pore volumes were also calculated using the Barrett-Joyner-Halenda protocol.20

X-Ray Diffraction

The XRD patterns of the samples were collected using an X-ray diffractometer (Thermo ARL, England) equipped with a CuKa target as a source for radiation at 30 kV and 30 mA. Data were obtained from small (0.7° to 10°) and wide $(2^{\circ} \text{ to } 50^{\circ})$ diffraction angles (2θ) with a

step size of 0.02° and a scanning speed of 4°/ min radiation. The average crystallite size was calculated from the XRD data using the Debye-Scherrer equation, as follows:21

$\tau = \frac{0.9\lambda}{\beta \cos\theta}$

where τ is the crystallite size, λ is the X-ray wavelength (1.54 [Å]), β is the full width at half maximum, and θ is the scattering angle of the (100) diffraction peak.

Dynamic Light Scattering

The particle size distribution of the MSNs in deionized water was determined using an in situ particle size analyzer (Microtrac, U.S.A.) based on 180° heterodyne light scattering and a proprietary controlled reference method.

Silibinin Loading onto Mesoporous Silica Nanoparticles

SBN was loaded onto the MSNs via the direct addition method. Briefly, the SBN solution in absolute ethanol was added to the MSNs and slowly mixed for 24 hours at 40 °C in different SBN/MSN weight ratios (0.07, 0.134, 0.2, 0.45, 0.7, 1, 1.4, 2, and 3). Immediately after the loading process, the particles were centrifuged at 12 000 rpm for 30 minutes. The equilibrium concentration of free SBN was assayed by ultraviolet-visible (UV-Vis) spectroscopy at a maximum wavelength (\lambda max) of 287 nm according to the standard curve plotted for standard solutions in the range of 5 to 200 µg/ mL. The loaded amount of SBN was determined directly after the MSNs were solubilized by adding 0.1 mL of hydrofluoric acid, which was thereupon diluted to 1 mL with absolute ethanol and detected via UV-Vis spectroscopy. Afterwards, the loading efficiency and the loaded SBN amount were calculated using the following equations:22

Loading efficiency (%) =

 $\frac{Amount of loaded silibinin (mg)}{Amount of the silibinin loaded (mg)} * 100$ Loaded amount (%) =

Amount of loaded silibinin (mg)

 $\overline{(Amount of loaded silibinin (mg) + Amount of MSN (mg))}$

* 100

Silibinin Adsorption Isotherms

The data on drug loading were fitted to various adsorption isotherms to explain the underlying mechanism of SBN adsorption onto the MSNs. Different adsorption models were utilized, Langmuir, Freundlich, including Dubinin-Radushkevich, and Temkin.23 In contrast to the Freundlich isotherm, which is used when heterogonous and multilayer adsorption occurs, the Langmuir isotherm explains homogeneous and monolayer adsorption with no interactions between the adsorbed molecules. The Dubinin-Radushkevich model is applied in multilayer adsorption phenomena with the Gaussian energy distribution onto heterogeneous surfaces. The Temkin model assumes the effects of indirect adsorbate/adsorbate interactions. The linearized forms of the model equations were drawn upon to verify the best-fitted model, as follows:23

Langmuir Equation: 1/qe=1/Ce×1/(k_L.qmax)+1/ gmax

Freundlich Equation: Log(qe)=Log(k,)+1/n×Log (Ce)

Dubinin–Radushkevich Equation: Ln (qe)=Ln (qmax)- $\beta \times \epsilon^2$, $\epsilon = R \times T \times Ln$ (1+1/Ce)

Temkin Equation: $qe=B_T \times Ln (K_T)+B_T \times Ln (Ce)$

where qe is the amount of SBN adsorbed per unit mass of MSNs (mg.g⁻¹), Ce is the concentration of unabsorbed SBN at equilibrium (mg.l⁻¹), qmax is the monolayer saturation capacity (mg.g⁻¹), K_L is the Langmuir constant related to adsorption capacity (mg.g⁻¹), K_f and 1/n are the respective Freundlich adsorption capacity and intensity, β is the Dubinin– Radushkevich constant, β is the Polanyi potential, R is the gas constant (8.31 J.mol⁻¹.K⁻¹), T is the absolute temperature (°K), B_T is the Temkin constant related to adsorption energy (J.mol⁻¹), and K_T is the Temkin binding constant (L.g⁻¹).

In Vitro Release Kinetics

The release of the loaded SBN from the formulation prepared with 6 mL of n-heptane and 0.5 mg/mL of MMA (H1M1), and the formulation prepared with 45 mL of n-heptane and 20 mg/mL of MMA (H2M2) was investigated in comparison with the equivalent amount of the free drug powder. Accordingly, an accurately weighed amount of each sample was dispersed in deionized water by

bath sonication and transferred into the dialysis tubing (cutoff=6-8 KD). The samples were transferred into the dialysis tubing (cutoff=6-8 KD) and immersed in 10 mL of a simulated gastric fluid (0.1N of the hydrochloric acid buffer solution, pH=1.2) and a simulated intestinal fluid (phosphate buffer [pH=6.8], containing 0.5% Pluronic F-127 to maintain sink condition) for 12 hours at 37 °C while shaking at 50 rpm. At predefined time intervals, an aliquot of 0.1 mL was withdrawn from the release medium and replaced by the same volume of the fresh medium. The SBN concentration in the release medium was determined by UV-Vis spectroscopy at a λ max of 287 nm. The cumulative percentage of SBN release was plotted against time. The kinetics of the drug release was analyzed by fitting the data through different mathematical models (zeroorder, first-order, Higuchi, Korsmeyer-Peppas, and Hixson-Crowell). The most appropriate model was chosen based on the R-squared (R^2), as was similarly reported in other studies.^{24, 25}

2, 2-Diphenyl-1-Picrylhydrazyl Free Radical Scavenging Activity

The free radical scavenging activity of SBN at different pH levels was determined by DPPH, a stable organic radical, which undergoes a color change from violet to yellow with H-donor antioxidants.²⁶ Accordingly, DPPH (2 mg) was dissolved in 20 mL of ethanol to make a stock solution. Thereafter, 200 µg/mL of free SBN or an equivalent amount of the SBN-loaded MSNs was dispersed in aqueous media at pH levels of 1.2, 4.5, and 6.8. An aliguot of the samples was incubated at 37 °C for 48 hours. Subsequently, 200 µL of 0.1 mM of the DPPH solution was added to 20 µL of the samples withdrawn at different time intervals and incubated in a dark room for 30 min. UV absorbance intensity was measured at 517 nm, and the antioxidant activity was calculated as inhibition (%) according to the following equation:27

Inhibition (%)= $(1-(A_{s}/A_{c})) \times 100$

where A_s and A_c are the absorbance of the sample and the control (SBN-free medium), respectively.

Statistical Analysis

Replicate data were expressed as the mean±SD (n=3). The statistical analyses were performed using the Prism software (version 5, GraphPad, USA). The physicochemical attributes of the formulations were compared using the one-way analysis of variance (ANOVA) and the Tukey *post-hoc* tests was used to evaluate the significant differences between the groups. In addition, at each pH level, changes



Figure 2: N₂ adsorption/desorption isotherms of the (A) H0M0, (B) H1M1, and (C) H2M2 are presented in different relative pressures. ADS: Adsorption; DES: Desorption; MMA: Methyl methacrylate; H0M0: A formulation prepared without adding n-heptane and MMA; H1M1: A formulation prepared with 6 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 6 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mg/mL of n-heptane and 0.5 mg/mL of MA



Figure 3: A) SBN amount (%) loaded onto the MSNs is shown as a function of the drug/MSN weight ratio. B) Cumulative drug release (%) was determined in the SBN-loaded H1M1 and H2M2 and the free SBN powder in acidic gastric juice (pH=1.2) for 2 hours and then in the phosphate buffer (pH=6.8) for 10 hours. SBN: Silibinin; MSN: Mesoporous silica nanoparticles; MMA: Methyl methacrylate; H1M1: A formulation prepared with 6 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 20 mg/mL of MMA

in the antioxidant activities of the samples (H2M2-loaded *vs.* free SBN) were compared between various incubation times using the repeated-measure ANOVA, while the sample was considered to be a covariate. P values of less than 0.05 were considered statistically significant.

Results

Morphology, Particle Size, and Pore Characterization of Mesoporous Silica Nanoparticles

MSN morphology and particle size were characterized by FE-SEM and DLS. As is shown in the FE-SEM micrographs (figures 1B

and C), the HIM1 and H2M2 samples similarly showed spherical particle morphologies with a cauliflower-like association. The DLS experiment results revealed that hydrodynamic sizes were roughly in the range of 25 to 100 nm, depending on the reaction condition (table 1).

The pore characteristics of the MSNs were determined from the N_2 adsorption/desorption isotherms (figure 2). Table 1 summarizes the BET analysis results. The pore sizes ranged from 2 to 7 nm, and the specific surface areas varied from 1200 to 600 m²/g.

Silibinin Loading

Figure 3A depicts the drug loading of the

H1M1 and the H2M2, indicating the higher loading of SBN onto the H2M2 in various weight ratios. In contrast to the control sample (H0M0), which showed only the drug loading of about 1%, the loading capacity increased to about 13% for the H2M2 at the SBN/MSN ratio of 2. The mechanism of drug loading was further elucidated by employing different adsorption isotherms to fit the experimental data. R^2 was used to select the best model (table 2), indicating that the Freundlich adsorption was the best-fitted model with R^2 of 0.95 for SBN adsorption similarly onto the H1M1 and the H2M2.

X-Ray Diffraction Pattern

The XRD experiment was first performed to investigate the order of the MSN pores at 2θ in the range of 0.7° to 10° (figure 4A), which confirmed a typical XRD pattern of MCM-41 with a 2D hexagonal symmetry for the H1M1 and the H2M2.²⁸ Individual intense peaks were found similarly at 2 θ around two for the H1M1 and the H2M2, which could be attributed to (100) reflection.

The possible changes in the physical state of SBN after loading onto the H2M2 were further investigated by repeating the XRD experiment, but for 20 in the range of 2° to 50° (figure 4B). It was evident that the free SBN powder showed diffraction peaks at 20 of 14.48°, 17.16°, 19.56°, 22.28°, 24.48°, and 26.82°. Some of the peaks

were sharp and intense, which indicated the crystalline nature of SBN. In contrast, the X-ray diffractogram of the SBN-loaded MSNs showed the complete disappearance of the characteristic crystalline peaks. The broad peak around 22° confirmed the existence of amorphous silica in the H2M2, as was similarly reported elsewhere.²⁹ Additionally, three small peaks at 20 of 2.34°, 4.14°, and 5.36° were observed, which were related to the characteristic (100), (110), and (200) reflections of the H2M2.³⁰

In Vitro Release

Figure 3B illustrates the SBN release profile of the H1M1 and the H2M2 compared with the equal quantity of the free drug powder. The results indicated that the SBN-loaded H1M1 and H2M2 comparably exhibited a typical sustainedrelease pattern over 12 hours and a significant (P<0.001) enhancement in SBN solubility compared with the free SBN powder. On the other hand, a more sustained drug release at early times, followed by a faster release, were noticed in the H2M2 formulation compared with the H1M1 formulation. The SBN release profiles were compared through the calculation of the mean dissolution time (MDT), the dissolution efficiency percentage (DE%), and the similarity factor (F2) (table 3). The F2 value was less than 50, and the MDT and DE% factors were found to be higher in the H2M2 than the H1M1.

Table 2: Adsorption isotherm parameters and correlation coefficients (R ²) for the H1M1 and the H2M2												
Sample	Langmuir			Freundlich		Temkin			Dubinin–Radushkevich			
	Q _m (mg/g)	К _L (L/g)	R ²	К _ғ (L/g)	n	R ²	Κ _τ (L/g)	B _τ (J/mol)	R ²	Q _s (mg/g)	K _D (mol²/kJ²)	R ²
H1M1	78.7	2.6×10 ⁻⁵	0.93	3×10-4	0.77	0.95	1.3×10 ⁻³	9.08	0.78	11.0	0.18	0.75
H2M2	286.4	2.3×10⁻⁵	0.93	1×10-3	0.76	0.95	1.3×10 ⁻³	28.5	0.81	35.1	0.18	0.76

MMA: Methyl methacrylate; H1M1: A formulation prepared with 6 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 20 mg/mL of MMA; R²: Correlation coefficients; Q_m : Monolayer saturation capacity; K_L : Langmuir constant; K_r : Freundlich adsorption capacity; n: Freundlich exponent; K_T : Temkin binding constant; B_T : Temkin constant related to adsorption energy; Q_s : Theoretical isotherm saturation capacity; K_0 : Dubinin–Radushkevich isotherm constant



Figure 4: Low-angle X-ray diffractograms were overlaid for the unloaded H1M1 and H2M2, and (A) wide-angle X-ray diffractograms were compared between the SBN-loaded H2M2, free SBN powder, and unloaded H2M2 samples (B). SBN: Silibinin; MSN: Mesoporous silica nanoparticles; MMA: Methyl methacrylate; H1M1: A formulation prepared with 6 mL of n-heptane and 0.5 mg/ mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 20 mg/mL of MMA

Table 3: Independent model parameters for the release of silibinin from the H1M1 and the H2M2								
Sample	MDT (h)	DE%	F2					
H1M1	2.87	64.8	21.6					
H2M2	3.15	71.8						

MDT: Mean dissolution time; DE%: Dissolution efficiency percentage; MMA: Methyl methacrylate; H1M1: A formulation prepared with 6 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 20 mg/mL of MMA; F2: Similarity factor (an index calculated for the H1M1 in comparison with the H2M2 or vice versa)

Table 4: Kinetic parameters for silibinin release from the H1M1 and the H2M2										
Zero-Order		First-Order		Higuchi		Korsm	Korsmeyer–Peppas		Hixson–Crowell	
K ₀	R ²	K,	R ²	K _H	R ²	N	R ²	К _{нс}	R ²	
14.48	0.95	0.49	0.83	33.6	0.98	0.57	0.96	0.29	0.96	
14.33	0.96	0.44	0.97	38.3	0.95	0.62	0.96	0.30	0.95	
	Zero K ₀ 14.48	Zero-Order K ₀ R ² 14.48 0.95	Zero-Order Firs K ₀ R ² K ₁ 14.48 0.95 0.49	Zero-Order First-Order K ₀ R ² K ₁ R ² 14.48 0.95 0.49 0.83	Zero-Order First-Order Hi K ₀ R ² K ₁ R ² K _H 14.48 0.95 0.49 0.83 33.6	Zero-Order First-Order Higuchi K ₀ R ² K ₁ R ² K _H R ² 14.48 0.95 0.49 0.83 33.6 0.98	Zero-Order First-Order Higuchi Korsm K ₀ R ² K ₁ R ² K _H R ² N 14.48 0.95 0.49 0.83 33.6 0.98 0.57	Zero-Order First-Order Higuchi Korsmeyer–Peppas K ₀ R ² K ₁ R ² K _H R ² N R ² 14.48 0.95 0.49 0.83 33.6 0.98 0.57 0.96	Zero-Order First-Order Higuchi Korsmeyer-Peppas Hixson K ₀ R ² K ₁ R ² K _H R ² N R ² K _{HC} 14.48 0.95 0.49 0.83 33.6 0.98 0.57 0.96 0.29	

MMA: Methyl methacrylate; H1M1: A formulation prepared with 6 mL of n-heptane and 0.5 mg/mL of MMA; H2M2: A formulation prepared with 45 mL of n-heptane and 20 mg/mL of MMA; R²: Correlation coefficients, K₀: Zero-order release constant; K₁: First-order rate constant; K_H: Higuchi dissolution constant; N: Release exponent; K_{Hc}: Hixson–Crowell rate constant

The mechanism of SBN release was investigated by fitting the release data in zeroorder, first-order, Higuchi, Korsmeyer–Peppas, and Hixson–Crowell mathematical models. As is presented in table 4, the Higuchi model was best fitted according to the model's R².

2, 2-Diphenyl-1-Picrylhydrazyl Free Radical Scavenging

The DPPH free radical scavenging assay was applied to determine the antioxidant activity of SBN at different pH levels. In contrast to the medium pH levels of 4.5 and 6.8, which did not cause any significant change in DPPH inhibition (%) (P=0.2), the antioxidant activity of free SBN decreased after exposure to acidic gastric juice (pH=1.2). Interestingly, the SBN-loaded H2M2 showed more antioxidant activity than free SBN at a pH of 1.2 (figure 5).



Figure 5: The figure shows the DPPH inhibition (%) of the silibinin-loaded H2M2 at a pH of 1.2 (A), pH of 4.5 (B), and pH of 6.8 (C), and free silibinin at a pH of 1.2 (D), pH of 4.5 (E), and pH of 6.8 (F) after incubation at 37 °C. DPPH: 2, 2-diphenyl-1-picrylhydrazyl; MMA: Methyl methacrylate; H2M2: A formulation prepared with 45 mL of n-heptane and 20 mg/mL of MMA; Replicate data were expressed as the mean±SD (n=3). DPPH inhibitions (%) were compared at a certain pH between the silibinin-loaded H2M2 and free silibinin using the one-way analysis of variance and the Tukey post-hoc tests was used to evaluate the significant differences between the groups.

Discussion

MSNs are routinely synthesized through the solgel reaction of silica precursors in the presence of soft-templating materials (e.g., CTAB).³¹ However, such syntheses are hampered by several issues such as small pore sizes and unfavorable pore morphologies for high-capacity drug loading. In the present study, we developed a one-pot synthesis method based on the combination of the sol-gel of the TEOS precursor and the radical polymerization of the MMA monomer in n-heptane/ water dispersion. Aiming to simultaneously tune the particle size and the pore diameter, we performed the reactions in different n-heptane volume ratios and MMA monomer concentrations. Interestingly, the particle sizes decreased in tandem with increases in the n-heptane volume, possibly because the n-heptane/water interface can adsorb particles and prevent their aggregation in the bulk medium, as was explained elsewhere,³² and it was shown that high concentrations of MMA resulted in larger pores, as was similarly described by Zhang and colleagues.³³ Moreover, the specific surface area decreased in parallel with increases in MMA concentrations due to the formation of larger pores.

We determined the pore characteristics of MSNs from N_2 adsorption/desorption isotherms. A hysteresis pattern indicates a porous silica structure. The International Union of Pure and Applied Chemistry (IUPAC) has classified the hysteresis pattern into four types: designated H1 to H4, which correspond to pore shapes.³⁴ Accordingly, the hysteresis pattern of the H0M0 sample mostly resembles type H1, which corresponds to cylindrical pores, whereas the hysteresis pattern of the H2M2 bears a resemblance to type H2 (ink bottle) pores. The H1M1 showed an intermediate property, indicating a shift from type H1 to H2 hysteresis pattern. The appearance of the H₂ pattern can

be due to the prevention of N_2 desorption from narrow-necked pores.³⁵

We loaded SBN, a poorly water-soluble phytochemical drug, onto the MSNs in different weight ratios of SBN to MSN, as was similarly studied for curcumin.19 Likewise, Cao and colleagues formulated porous silica nanoparticles reverse microemulsion via the method, which showed only 5% silymarin loading (the standardized extract of milk thistle seeds).³⁶ Fazio and colleagues prepared a system composed of poly(ethylene glycol)-poly(lactic-co-glycolic acid)-Au (PEG-PLGA-Au), which showed about 8.8% SBN loading.37 The high capacity loading of SBN in the H2M2 (13%) compared with that in the mentioned studies confirms the suitability of the MSN carrier for SBN delivery.

The amount of the loaded SBN was influenced by the pore size, indicating the high loading capacity of the H2M2, with the mean pore size of 7 nm, in comparison with the control sample (H0M0), with the mean pore size of 2 nm. Although the H2M2 provided a lower specific surface area for SBN adsorption, its larger pores impeded the SBN transport into and out of the pores less; hence, we attained higher SBN loading with the H2M2. The Freundlich adsorption was the best-fitted model in SBN adsorption similarly on the H1M1 and the H2M2 particles. This model is generally used to describe heterogonous and multilayer adsorption phenomena.²⁹ Interestingly, the high K, calculated for the H2M2 compared with the H1M1, indicated increased adsorption capacity by the MSNs with larger pore diameters. In addition, 1/n values of greater than 1 were indicative of S-type isotherms, which are commonly observed for the compounds containing polar functional groups.38 At low adsorbate concentrations, it appears that ethanol can compete with SBN, which results in low-affinity adsorption. However, with increasing SBN concentrations, the surface adsorption initially increases and eventually decreases until it becomes zero as vacant adsorbent sites are thoroughly filled.39

To investigate the order of the MSN pores, we performed the XRD experiment at 20 in the range of 0.7° to 10°. The peak positions 100 at 20 were less than 2.5° (corresponding to the average d-spacing=4.4 nm), indicating mesoporous materials.⁴⁰ In addition, the crystallite size was calculated to be 15.4 and 13.8 nm in the H1M1 and the H2M2, respectively. The reflections of 110 and 200 were not easily seen in the obtained diffractograms, which can be due to their very low intensity, which is in the same line with a previous study.⁴¹ To further investigate the possible changes in the physical state of SBN after loading onto the H2M2, we carried out the

XRD experiment for 20 in the range of 2° to 50°. Unlike the X-ray diffractogram of the free SBN powder, which showed some sharp and intense peaks of the crystalline SBN powder, as was reported by Patel and colleagues,¹⁷ the SBN loaded onto the MSNs presented the complete disappearance of such peaks, suggesting the formation of amorphous SBN after loading onto the MSNs, probably due to the suppression of drug crystallization in the confined mesopores of the H2M2, as was similarly explained by Patel and others¹⁷ and Sahibzada and colleagues.⁴²

The SBN release profile showed that both SBNloaded H1M1 and H2M2 formulations provided a typical sustained-release pattern over 12 hours and significantly enhanced drug dissolution, by comparison with the free SBN powder. Similarly, Patel and colleagues prepared shellac colloidal particles containing SBN, which showed a 90% release rate over 4 hours.¹⁷ In another study, Cao and others showed a very sustained release of silymarin from porous silica nanoparticles (about 13% after 72 h).³⁶ In addition, Lu and colleagues formulated hydroxypropyl methylcellulose matrix tablets, which showed a 20% SBN release rate over 12 hours.43 It seems that the enhanced SBN dissolution, as is shown in the present study, can be due to not only the conversion of the crystalline SBN powder into the microcrystalline or amorphous state via loading onto mesopores, as was demonstrated in the XRD diffractograms, but also the formation of large mesopores in the silica matrix, which enhanced the SBN transport out of the particles. Furthermore, with respect to the F2 value, which was calculated to be less than 50, we did not consider the release profiles to be similar. Importantly, we found higher MDT and DE% factors in the H2M2 than the H1M1, which can be explained by the large ink-bottle pores in the H2M2, as was explained before. As is presented before, it was difficult for us to choose the proper release kinetic model owing to the close similarity of R² in different models. The Higuchi model fitted the release data, confirming that passive diffusion was involved in SBN release from the insoluble matrix, as was similarly explained elsewhere for MCM-41 nanoparticles.⁴¹ The rate constant (K_H) was determined to be higher for the H2M2 than the H1M1, which can be due to the larger pores of the H2M2. The underlying mechanism of SBN release was investigated through the calculation of the Korsmeyer-Peppas release exponent (n): the calculated figure was between 0.45 to 0.89, indicating that the drug release deviated from the Fickian diffusion.44 Such a deviation from the classical passive diffusion mechanism can be explained by the slow degradation of the amorphous silica matrix over time, as was explained elsewhere. $^{\rm 45}$

The sustained release of SBN from the H2M2 resulted in a more retained DPPH free radical scavenging activity of SBN in the supernatant than the free powder SBN, which was significantly apparent at a pH of 1.2. Mean differences in DPPH inhibition (%) were determined to be 5.18%±2.13%, 1.05%±1.84%, and 1.59%±0.74% at pH levels of 1.2, 4.5, and 6.8, respectively. Similarly, Patel and colleagues reported that shellac colloidal particles attenuated SBN degradation at a pH of 1.2.17 Moreover, it was reported that SBN dimers could be formed by phosphodiester bonds between -OH groups after exposure to the phosphate buffer,¹⁵ which can explain the preservation of SBN activity in this medium (pH=6.8) in comparison with acidic gastric juice (pH=1.2).

Conclusion

In the present study, a new preparation method was developed for the synthesis of MSNs to enhance the loading and dissolution of poorly water-soluble phytochemicals (e.g. SBN). This preparation method shares the features of the simultaneous free-radical polymerization of the MMA monomer and the sol-gel reaction of the silica precursor (TEOS) at the n-heptane/water interface. Pore sizes and particle diameters were drastically affected by changing the monomer concentration and the n-heptane/water volume respectively. FE-SEM micrographs ratio. showed that the MSNs had a spherical shape. The BET analysis results confirmed the control of the pore size and the specific surface area in the range of 2 to 7 nm and 600 to 1200 m^2/g , respectively. The DLS data disclosed that the different volumes of n-heptane resulted in different particle sizes, ranging from 25 to 100 nm. Interestingly, SBN loading was pore-size dependent in that it changed from 9 to 13% w/w in the MSNs with the pore size of 5 and 7 nm, respectively. Our in vitro release study indicated that, unlike free SBN, which exhibited extremely low dissolution efficiency, the SBN-loaded MSNs offered a typical sustained-release of about 90% over 12 hours. Concurrently, better preservation of SBN in the acidic gastric pH (1.2) was attained via loading onto the H2M2. Altogether, welltuned MSNs can confer poorly water-soluble phytochemicals such as SBN sustained release, augmented preservation, and enhanced oral bioavailability. Finally, further in vitro and in vivo investigations are needed to study other aspects of this formulation; for example, the possible toxicity of MSNs and the residual MMA monomer.

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